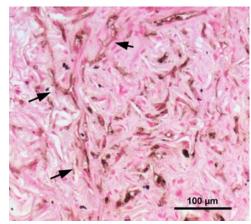


# Characteristic Quantities of Microvascular Structures in CLSM Volume Datasets

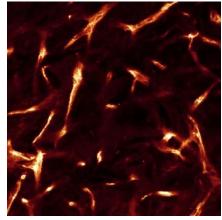
K. Winter<sup>1</sup>, L. H.-W. Metz, J.-P. Kuska<sup>2</sup>, B. Frerich<sup>3</sup>

<sup>1</sup>Translational Centre for Regenerative Medicine (TRM-Leipzig), University of Leipzig, <sup>2</sup>Interdisciplinary Centre for Bioinformatics (IZBI), University of Leipzig, <sup>3</sup>Department of Oral and Maxillofacial Surgery, University of Leipzig

- Models for "microvascular engineering" in vitro
  - Long term goals
    - Integration of a supplying vessel construct ("feeder donor vessel")
    - Functional microvascular networks
  - Short term goals
    - Models, imaging, quantification
    - Functional analysis (ESR, oxygenation, pH, etc.)



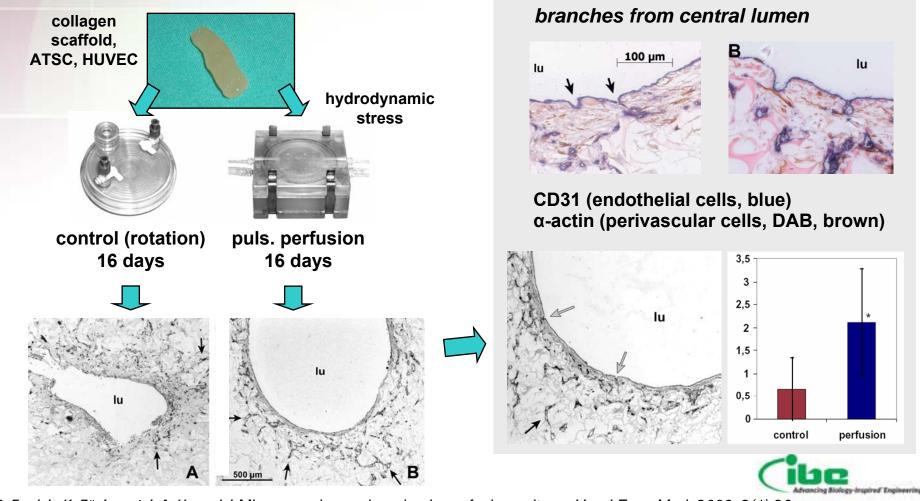
Histologic section, CD31 (DAB, brown)



Confocal laser scanning microscopy (CLSM), UEA-TRITC

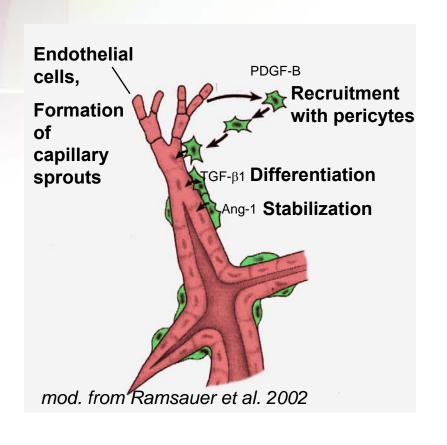


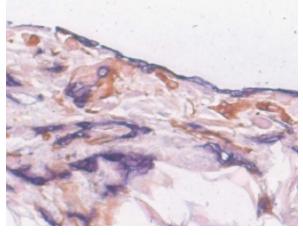
3D in vitro vessel model with capillary structures

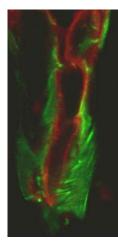


B. Frerich, K. Zückmantel, A. Hemprich Microvascular engineering in perfusion culture. Head Face Med, 2006; 2(1):26

Stabilization and maturation of newly formed capillaries





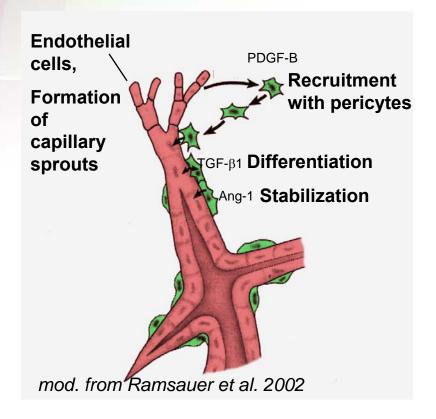


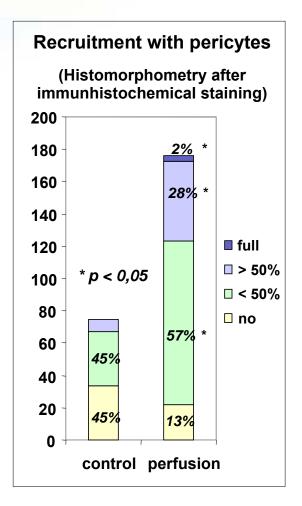
Morphological parameters, e.g.

- Recruitment with  $\alpha$ -actin-positive cells
- Length, information about microvascular networks
- → Histomorphometry
- → Image analysis of CLSM-data



 Stabilization and maturation of newly formed capillaries



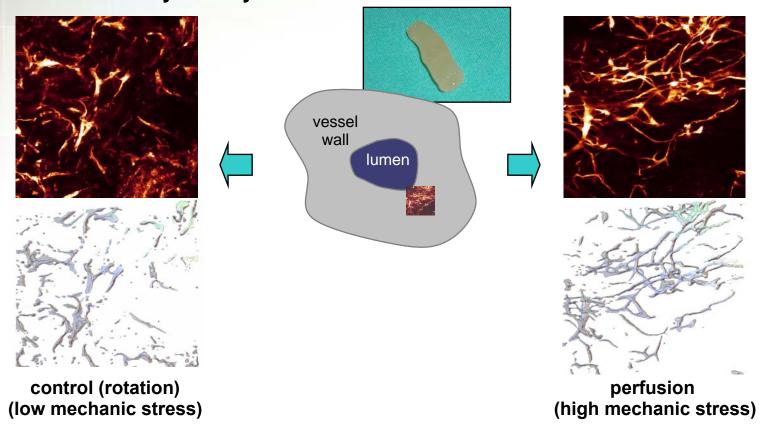


B. Frerich, K. Zückmantel, S. Müller, A. Hemprich Maturation of capillary-like structures in a tube-like construct in perfusion and rotation culture. Int J Oral Maxillofac Surg, accepted and in press

dvancing Biology-Inspired Engineering

### 3D non-destructive imaging with CLSM

Influence of hydrodynamic stress on vessel formation



Need for comprehensive quantification



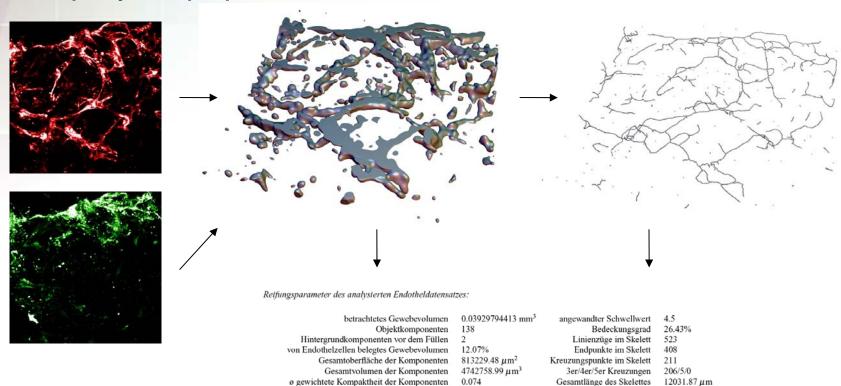
#### Quantification

- Method for fully automated morphological and topological analysis of microvascular structures
  - Calculation of several "characteristic quantities" for characterization and comparison of microvascular networks
  - Degree of vessel maturation and stability, recruitment with perivascular cells
  - Extracted c.q. provide information for advanced tissue engineering, in vitro angiogenesis and vessel formation of metabolically active tissues



### Quantification

Step-by-step quantification of CLSM datasets



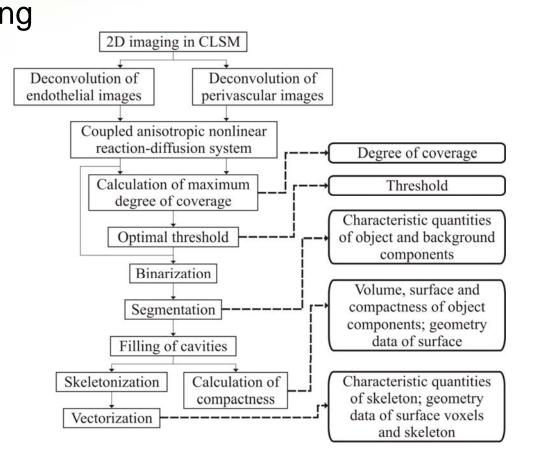
Daten der zehn größten Komponenten des Endotheldatensatzes:

Voxelanzahl	Volumen in $\mu$ m <sup>3</sup>	Fläche in $\mu$ m <sup>2</sup>	Kompaktheit	Gesamtlänge in $\mu$ m	Linien	Endpunkte	Kreuzungen	3er	4er
938326	3469706.06	544557.96	0.0084	8835.23	302	102	166	162	4
69386	254327.19	35701.47	0.1608	537.03	35	18	17	16	1
56487	208179.71	36600.85	0.1	584.31	21	9	11	11	0
48270	179126.11	24548.48	0.2453	195.25	5	4	2	2	0
42112	155727.83	24428.81	0.1881	230.49	5	4	2	2	0
13504	50668.29	9196.85	0.3733	94.39	3	3	1	1	0
12033	43649.36	12484.98	0.1107	219.46	3	3	1	1	0
11714	41914.83	11980.93	0.1155	210.33	7	5	3	3	0
7219	26820.68	6467.85	0.3007	69.13	5	4	2	2	0
7503	26028.96	8044.54	0.1472	151.93	5	4	2	2	0



#### Quantification

- Series of image processing steps for fully automatic image analysis and extraction of characteristic quantities from CLSM datasets
- Visualization of endothelial structures





### **Image preprocessing - Deconvolution**

- Image quality suffers from optical aberration, a wide range of noise sources (detector noise, laser noise, shot noise of the light) and shading effects
- Mathematical interpretation: convolution of the source signal (actual image) with an interfering signal (PSF of the CLSM)

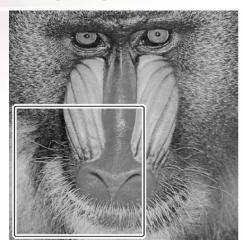
$$B(\vec{r}) = O(\vec{r}) \otimes PSF(\vec{r})$$

- Restoration of the original image by deconvolution
- Implementation of the Richardson-Lucy deconvolution algorithm

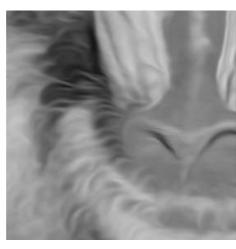


# Image preprocessing - Coupled anisotropic nonlinear reaction-diffusion system

- Removes noise from datasets and strengthens thin endothelial and perivascular structures
- Preservation of edges since diffusion occurs perpendicularly to grayscale gradients





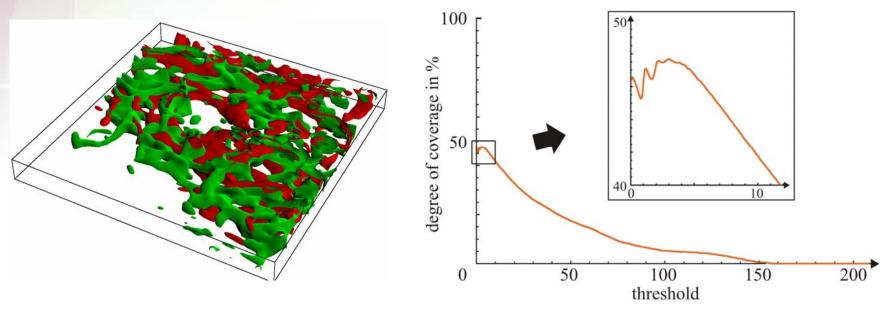


isotropic (middle)
vs. anisotropic (right)
nonlinear diffusion

 Spatial separation of endothelial and perivascular structures by means of a catalyzed decomposition instead of a simple masking operation

# Image analysis – Recruitment with perivascular cells

 Computation of the real contact surface of endothelial and perivascular structures by using a variable threshold



 Maximum degree of coverage corresponds to the optimum threshold for subsequent segmentation of the endothelial dataset



### Image analysis - Compactness

- Important characteristic morphological quantity
- Computation of surface and volume from segmented data with a modified Marching Tetrahedron algorithm

$$C = \frac{36\pi V^2}{S^3}$$

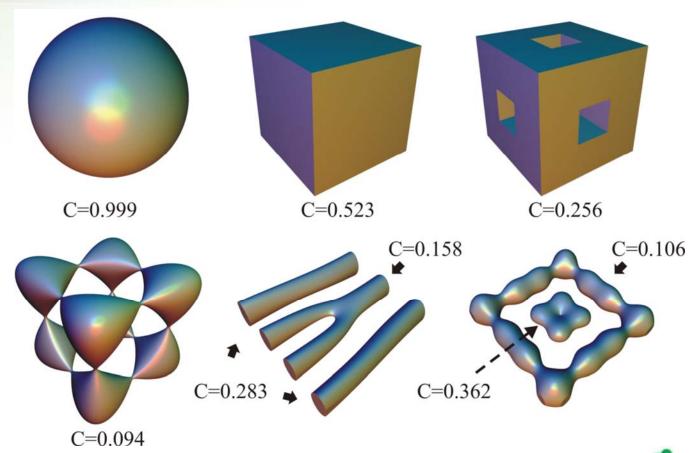
$$C_{\emptyset} = \sum_{n=1}^{\#OC} \frac{C_n \times V_n}{V_{tot}}$$

Triangulation of the threshold depending iso-surface provides data for visualization



### **Image analysis – Compactness**

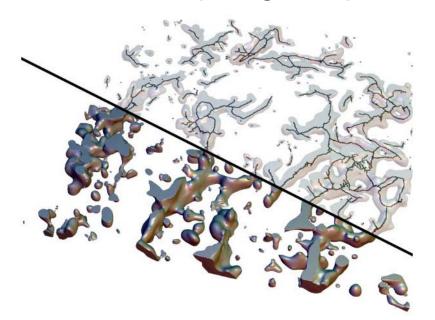
Some synthetic objects and their compactness





# Image analysis – Skeletonization and vectorization

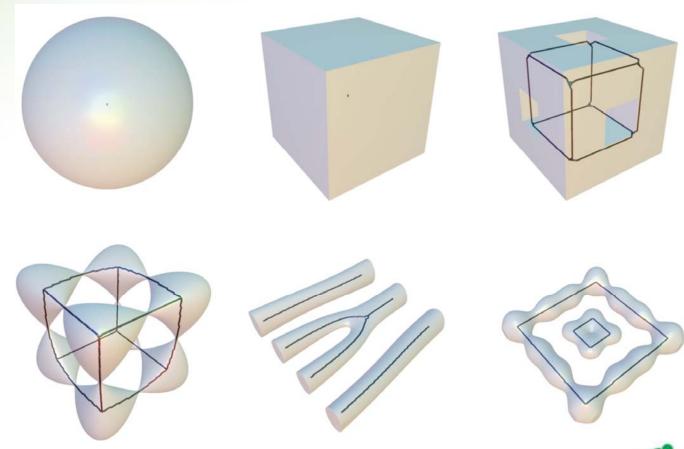
- Development of an anisotropic skeletonization algorithm for segmented endothelial data, location of medial axes
- Computation of length and identification of junction / line end points of the skeleton
- Analysis of connectivity and branching
- Important characteristic topological quantities





# Image analysis – Skeletonization and vectorization

Some synthetic objects and their skeleton



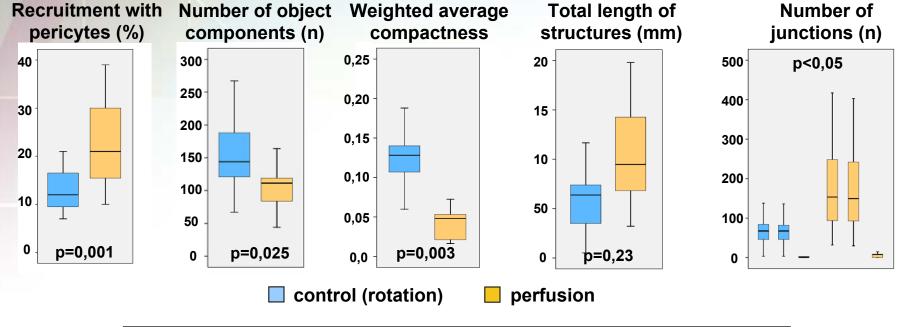


## **Characteristic quantities**

<u> </u>	The state of the s
Symbol	Description
%DC	Maximum degree of coverage
$\theta$	Threshold
#OC	Number of object components
#BC	Number of background components
V	Volume of a single component
${ m V}_{tot}$	Volume of all components
S	Surface of a single component
$\mathrm{S}_{tot}$	Surface of all components
C	Compactness of a single component
$C_\emptyset$	Average weighted compactness of all components
#LEV	Number of line end voxels of a single component
$\# \text{LEV}_{tot}$	Number of line end voxels of all components
#JV	Number of junction voxels of a single component
$\# { m JV}_{tot}$	Number of junction voxels of all components
#LS	Number of line segments of a single component
$\#LS_{tot}$	Number of line segments of all components
L	Length of a skeletonized component
$L_{tot}$	Length of all skeletonized components



#### Results



characteristic quantity	p-value	characteristic quantity	p-value	
%DC	0.001	$L_{tot}$	0.230	
heta	0.679	$\# LS_{tot}$	0.311	
#OC	0.025	$\# LEV_{tot}$	0.200	
#BC	0.830	$\# \mathrm{JV}_{tot}$	0.034	
${ m V}_{tot}$	0.936	$\#JV_3$	0.041	
$\mathrm{S}_{tot}$	0.522	$\# \mathrm{JV}_4$	0.033	
$C_\emptyset$	0,003			



#### Conclusion

- Method for analysis and visualization of microvascular structures in CLSM volume datasets
- Algorithms are universal, they can be used for quantification of other structures and networks from different modalities (i.e. macrovascular structures, neurites, airways, etc.)
- Extracted characteristic quantities are transferable and can be used to analyze multimodal volumetric datasets
- Also allow comparison of arbitrary structures to each other



### **Acknowledgements**







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Thanks for your attention!

